Accommodative holography: improving accommodation response for perceptually realistic holographic displays - Supplementary Material

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S1 ADDITIONAL DETAILS ON IMPLEMENTATION

System

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20 Figure S1 shows an overview of the benchtop prototype utilized in the experimental evaluations. The fiber-coupled laser 21 diode (LD, Wikioptics) emanates a full-color beam with the wavelength of 638 nm, 520 nm, and 450 nm. A consecutive 22 placement of an objective lens (OL) with a numerical aperture of 0.25 (Newport, M-10X) and a collimating lens (CL) 23 with a focal length of 100 mm (Zeiss, Milvus 100 mm, f/2) collimates the laser beam with high uniformity. As mentioned 24 25 in Section 5.1, a FLCoS SLM and an LCoS SLM provided with the corresponding CGHs are optically relayed with a 26 series of lenses, respectively. In the optical arm of FLCoS SLM, the relay optics, which consist of L1 (Nikon, 135mm, 27 f/2.8) and L2 (Nikon, AF-S VR MICRO NIKKOR 105mm, f/2.8), effectively modifies the pixel pitch of FLCoS SLM (Fourth 28 Dimensional Displays, a resolution of 1920×1200 , a pixel pitch of 8.2μ m) to 6.4μ m in the relayed field. A physical 29 30 filter (F1) that blocks high-order signals and eventually determines the eye-box of the near-eye display is designed as a 31 rectangle with a size of 7.4 mm × 3.7 mm and modeled with a 3D printer is placed at the Fourier plane. On the contrary, 32 the LCoS SLM is relayed with lenses (L3, L4) of an identical model (Nikon, AF-S VR MICRO NIKKOR 105 mm, f/2.8) and 33 the filter (F2) with a size of 7.4 mm \times 3.7 mm. The OLED panel of BOE (0.39 inch, resolution of 1920 \times 1080) is 1.5 times 34 35 expanded to match the window size with two different achromatic doublets (L5: Thorlabs, AC508-100-A, L6: Thorlabs, 36 AC508-150-A) and the size of the filter (F3) is determined as 10.5 mm × 5.3 mm to match the effective size of eye-box 37 with the holographic displays. 38

The beams merged with multiple beamsplitters (BS) are again relayed with a 4-f system constructed with two identical achromatic doublets (L7, L8: Thorlabs, AC508-150-A). At the Fourier plane, a focus-tunable lens (FTL, Optotune

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Fig. S1. Overview of the benchtop prototype utilized in the experimental evaluations, the enlarged views of each section (red, orange) with the labeled components, and the inset that describes the classifications of individual components. In the enlarged photographs, the beam paths are colored white to show how the individual displays are visualized. The dashed lines in red, brown, green, blue, purple, and white respectively represent the display device, sensor, lens, mirror, synchronization module, and the other optics to construct the whole system. The auxiliary devices used in the user experiments, such as an eye occluder and a keypad, are highlighted with a yellow dashed line. For the lenses (L), filters (F), and shutters (S), additional indices are provided for convenient reference.

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EL-16-40-TC-VIS-5D-C) is placed to change the axial depth of the reconstructed image and controlled with the calibrated analog signal generated by a data acquisition board (National Instrument, USB-6343). The FTL is placed parallel to the ground to alleviate the aberration due to a gravitational force. The height of the whole display system is adjusted to an eye-level by putting a periscope (Newport) equipped with two flat mirrors. After beams are deflected with two mirrors, a 1-inch eyepiece lens (EL, Thorlabs, AC254-075-A) with a focal length of 75 mm is placed to virtually floating the image. The overall eye-box of the near-eye display system is provided as 5.27 mm × 2.64 mm, and the field of view is $7.8^{\circ} \times 4.4^{\circ}$.

For the accommodation experiments, the power refractor of Plusoptix (PowerRef3) measures an eye's refractive power with a speed of 50 Hz. The projection distance is given as 1.0 m from the eye, and a series of hot mirrors (Edmund Manuscript submitted to ACM Accommodative holography: improving accommodation response for perceptually realistic holographic displays -Supplementary Material

105 optics, #64-472) and a cold mirror (Edmund optics, #64-449) is placed for robust capture of one's retina with infrared 106 light. For full-color holographic displays, the TTL signals generated by each SLM are actively switched with two electric 107 switches (LCoS switch, FLCoS switch) attached to the main circuit to provide a single TTL signal to the LD engine. 108 109 Here, the shutters (S1, S2) and the connected controllers are also synchronized with the corresponding switches for 110 automated pairwise comparisons with a single LD source. The entire system is managed with an Arduino Uno board. 111 The images are captured with a charge-coupled device (CCD) (FLIR, GS3-U3-91S6C) having a resolution of 3376 × 2704 112 and a pitch of 3.69 μm at the IP. The dioptric distance of 0.6 D is converted to 2.8 mm, and the CCD is translated with 113 114 the help of the motorized linear stage (Newport, FCL100). We additionally equipped an eye occluder to block the other 115 eye during accommodation experiments, and a keypad to enter user response in preference experiments.

Apparatus

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The optical powers of the individual holographic scenes are measured with the optical power detector (Newport, 918D-SL-OD3R) with a circular aperture of 11.3 mm connected to the power meter (Newport, 2936-R) as shown in Fig. S1. The light fluxes of two holographic displays are balanced by placing NDFs with different transmittance ratios. The averaged optical powers of the reconstructed scenes (lion, market, castle, and castle with a Maltese cross) in red (638 nm), green (520 nm), blue (450 nm) channel are measured as 1.6 nW, 1.8 nW, and 2.5 nW, respectively. The converted luminance is estimated as 0.2 cd/m^2 , which is far below the permissible level of laser exposure.

Off-axis holographic displays

It is well known that the undiffracted lights are inherently present in on-axis holographic displays due to the finite fill 130 factor of SLMs. For example, the phase-only SLM (Holoeye, LETO-3 CFS-127) used in our experiments has a fill factor 132 of 93 %. The undiffracted light can be harmful to the user's eye when directly viewing the holographic display and can 133 hardly be managed in an on-axis configuration. Thus, we vertically rotated both SLMs in half of the diffraction angle 134 of the blue signal to eliminate the potential risk. Accordingly, the bandwidths of CGHs are also vertically-halved and 135 shifted to reconstruct the off-axis holographic image.

Automated pairwise comparisons

140 The holograms were provided by Holoeye's built-in SDK for LCoS SLM and OpenGL codes for FLCoS SLM. For FLCoS 141 SLM, the binary holograms are encoded to 24bit images where a single bit can contain a single binary hologram. 142 The encoded holograms are loaded on the graphics processing unit (GPU) with OpenGL for fast update of CGHs 143 with a maximum frequency of 150 Hz. When an image is reconstructed with a single SLM, the optical path of the 144 145 counterpart SLM is blocked by the optical shutter placed at the beam path, and these shutters are electrically controlled 146 by the Arduino Uno board. Similarly, the electrical switches are utilized to provide the illumination sequences of the 147 corresponding SLM depending on the trigger provided by the Arduino Uno board as the transistor-transistor logic 148 (TTL) signals of two SLMs are in different forms. 149

150 The pairwise comparison experiments were performed in a fully-automated manner. The entire experiments were 151 performed with a subject-dependent pre-defined csv file that contains a sequence of options and the user's answers 152 were saved in the corresponding file. Subjects were instructed to enter a response after a beep sound indicating that 153 both options were displayed. If an input other than the desired ones was given, another beep was played to re-enter the 154 155 response. 156

157 S2 ADDITIONAL EXPERIMENTAL RESULTS

159 Captured results

Other than the photographs of holographic images shown as Fig. 6, we additionally provide the captured results (focused, defocused) of three different CGH algorithms (B-SGD, DOF-opt B-SGD ($\gamma = 0.01$), DOF-opt B-SGD ($\gamma = 0.1$)) with six different temporal multiplexing conditions (TM=1, 2, 4, 8, 16, 24) as Fig. S2-S4. They are provided with three different images (lion, market, and castle) employed in the subjective image quality evaluations. In the bottom right corner of the focused images, the measured PSNR values are provided. As the regularization coefficient increases, the measured PSNR decreases, and the edges of the individual images get enhanced.



Fig. S2. Captured results of lion scene utilized in the subjective image quality evaluation. Image sources from DIV2K dataset [Agustsson and Timofte, 2017].

Tolerance of CGHs on the artifacts

In the user experiments performed to evaluate the subjective image quality, some participants reported that the moving artifacts are present in 8bit-SGD images, although we provided the images as shown in Fig. 6. The noticeable artifact led to relatively low JOD with large deviations across the subjects. We speculate the artifact roots from the dirt or debris inherently present in the optical system. Thus, we additionally placed a slide glass with small dirt on it in either the pupil plane or the image plane of the holographic displays to simulate this phenomenon. Then, we captured results at the image plane with the CCD camera as shown in Fig. S5.

As shown in Fig. S5, the holographic images of B-SGD and 8bit-GS showed the robustness to the artifacts that can be present in the optical system. However, the 8bit-SGD images showed little tolerance to the artifacts, and the defects with small ringing patterns get noticeable in the smooth sections of individual images. The images were highly susceptible to the minute movement of the slide glass as shown in 8bit-SGD with dust#1 at pupil and 8bit-SGD with dust#2 at pupil. If the artifacts are present in the pupil plane, the defects contain color fringes, easily noticeable in the actual experiments. Manuscript submitted to ACM

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Fig. S3. Captured results of market scene utilized in the subjective image quality evaluation. Image sources from DIV2K dataset [Agustsson and Timofte, 2017].



Fig. S4. Captured results of castle scene utilized in the subjective image quality evaluation. Image sources from DIV2K dataset [Agustsson and Timofte, 2017].

This issue can be handled with the recently introduced camera-in-the-loop calibration method [Chakravarthula et al., 2020, Peng et al., 2020] pre-compensating the artifacts with captured images only when the artifact is present in the display optics. The human eye consists of liquid layers and the tear film, which is the very outer part of the eye, is a complex mixture of lipids of different classes [Bron et al., 2004] that may result in undesirable diffraction Manuscript submitted to ACM



Captured results of focused images

Fig. S5. Captured results of holographic images acquired with various CGH algorithms to test the tolerance on the artifacts. Image sources from DIV2K dataset [Agustsson and Timofte, 2017].

and interference. Moreover, human eyes always move even when they are fixated. This raises the question that CGHs reproducing a coherent field with a narrow angular spectrum may not be suitable for practical use in holographic displays, although they demonstrate a superior quality with a single frame in the camera-captured results. Manuscript submitted to ACM Accommodative holography: improving accommodation response for perceptually realistic holographic displays -Supplementary Material

Results of accommodation experiments

The accommodation responses when viewing the holographic near-eye display prototype providing various CGHs are measured, and the additional results are presented as Fig. S6. Fig. S6(A) demonstrates the normalized accommodative gains averaged across the 21 subjects. They are provided depending on the number of TM frames as speckle reduction showed a strong correlation to the accommodative gain. Finally, we demonstrate the measured accommodation of individual subjects, including the dioptric amplitude estimated when viewing OLED as Fig. S6(B).

323 Change in pupil size

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During the accommodation experiments, we also measured the pupil diameter of users. Figure S7 demonstrates the pupil diameter measured when the subjects view the visual stimulus provided by OLED. We provide pupil diameter change for six cycles of 6 subjects who achieved the highest gains in the experiments. Some subjects showed consistency in the measured pupil size, while others showed noticeable differences over time and trials, although they viewed an identical visual stimulus. This inconsistency of pupil size indirectly indicates that CGH optimization based on one's eye model is hardly practical, especially when the pupil serves as a passband filter.

S3 ADDITIONAL SIMULATION RESULTS

Change in pupil size and its effect on holographic image quality

Since the primary goal of our work is to investigate the accommodation response through holographic near-eye displays,
 our prototype is built to have a sufficiently wide eye-box. The bandwidth is additionally halved in vertical directions
 to match the eye-box size of holographic near-eye displays built with two different SLMs. Moreover, the eye pupil
 functions as a finite passband preventing the holographic signal from entering the human eye. These practical issues
 have affected the quality of reconstructed image and further influenced the experimental evaluations.

To understand the effects of band-limitation on image quality in holographic near-eye displays, we demonstrate 343 the reconstructed images when the display parameter differs, and the pupil size varies as shown in Fig. S8. The 344 345 reconstruction is conducted with the specification of a phase-only SLM (a resolution of 1920×1080 , a pixel pitch of 346 6.4 µm) utilized in our work. We provide the retinal images of two CGHs (8bit-SGD and 8bit-GS) reconstructed under 347 two different eyepiece lens settings (a 2-inch lens with a focal length of 40 mm and 75 mm), two band-limitation types 348 (halved and whole), and three pupil diameters (pupil diameter of 3 mm, 5 mm and 7 mm). Recall that our prototype 349 350 utilizes an eyepiece lens with a focal length of 75 mm, and bandwidth is vertically halved. The images demonstrated in 351 Fig. S8 imply that the holographic images are susceptible to the eye-box of the near-eye display and the changes in 352 pupil size. In addition, the image quality is relatively consistent to the change in size of eye pupil when the eye-box of 353 holographic near-eye display is sufficiently small unlike ours. 354

Comparison to Neural 3D holography [Choi et al., 2021]

Choi et al. [2021] recently introduced the adoption of alternating direction method of multipliers (ADMM) solver to acquire phase-only CGHs to ensure piecewise phase smoothness of reconstructed complex-valued field. Smoothed phase leads to less speckle noise in the reconstructed holographic image. The proximal gradient solvers are known to effectively reduce the loss function that consists of l_2 and l_1 norm [Bach et al., 2012]. We provide the simulation results of GS, SGD, and ADMM CGHs in Fig.S9. Both focused and defocused holographic images of ADMM CGHs are similar Manuscript submitted to ACM



Fig. S6. Additional results of accommodation experiments. (A) Average of normalized accommodative gains measured when viewing various CGHs (8bit-SGD, 8bit-GS, B-SGD, DOF-opt B-SGD (γ =0.01), DOF-opt B-SGD (γ =0.1)). For the binary holograms (B-SGD, DOF-opt B-SGD (γ =0.01, 0.1)), holograms are realized with several TM conditions. The error bars indicate the standard error of the normalized accommodative gain measured depending on individual users. (B) Individual accommodation responses of 21 subjects are presented with the dioptric amplitudes of the fitted sinusoids. The results are sorted with the mean dioptric amplitude measured when viewing OLED (black). The dioptric amplitudes of each cycle are demonstrated with colored circles, and the excluded data are marked with additional stars.

to SGD CGHs. At the same time, the phase profile of the reconstructed field is proportionally smoothed in the case of the CGH with an ADMM solver.

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Fig. S7. Measured pupil diameter of six subjects who demonstrated highest gains with OLED viewing conditions. Each line represents a single cycle of 20 seconds.



Fig. S8. Effect of band-limitation on image quality in Fresnel-type holographic near-eye displays in simulation. The retinal images of 8bit-SGD and 8bit-GS holograms were reconstructed with different eyepiece lens (EL) settings (red, green), and different pupil conditions (pupil diameter of 3 mm, 5 mm, and 7 mm) are provided. In the right bottom corner, the signal's bandwidth is demonstrated as an inset. The eye pupil acts as a finite passband limiting the holographic signals. Image sources from DIV2K dataset [Agustsson and Timofte, 2017].

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Fig. S9. Simulation results of GS, SGD, and ADMM CGHs reconstructing a single 2-D image of castle scene. We demonstrate the intensity (1st row) with additional PSNR/SSIM in the right bottom and phase profile (2nd row) with mean of magnitude of laplacian of phase at the reconstructed image plane. In addition, the intensity profiles of retinal images in the focused state (3rd row) and two different defocused states (4th row: 0.6 D and 5th row: 1.0 D) reconstructed under a pupil diameter of 3 mm are provided with additional enlargements. SGD and ADMM CGHs visualize similar focused and defocused images, while a slight difference in phase smoothness between the two images is present. Image sources from DIV2K dataset [Agustsson and Timofte, 2017].

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S4 PSEUDOCODES OF CGH ACQUISITION ALGORITHMS

In this section, we provide the pseudocodes of CGH acquisition algorithms. For GS, SGD, ADMM algorithms, refer to [Choi et al., 2021, Gerchberg, 1972, Peng et al., 2020], respectively. We provide pseudocodes of Fresnel-type B-SGD [Lee et al., 2022] CGH acquisition algorithm as Algorithm 1. The binary hologram optimization procedure with contrast ratio regularization (DOF-opt B-SGD) proposed in this work is outlined as Algorithm 2.

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1:	slm : Pattern of binary SLM		
2:	Niter : Number of iteration		
3:	<i>I</i> : Number of frames for TM		
4:	α : Learning rate		
5:	$q(\cdot)$: Decoding operator for binary SLM		
6:	$\mathcal{P}_d(\cdot)$: Propagation of d		
7:	$\int a(\cdot, \cdot) : l_2 \text{ loss of amplitude}$		
y. 8.	$\mathcal{L}_{a}(\cdot)$ sRGB gamma correction operator		
0. 0.	hand $\operatorname{limit}(\cdot)$ · Band $\operatorname{limitation}$		
	$\Gamma_{\rm rest}$ band initiation $\Gamma_{\rm rest}$ $\Gamma_{\rm rest}$ $\Gamma_{\rm rest}$		
10:	$a_{target} \leftarrow \text{Load target amplitude with } \sqrt{1 \left(\frac{1}{target} \right)}$		
11:	for $j = 1 \dots J$ do		
12:	$\phi_{rand} \leftarrow \text{initialize phase in a range of } (-\pi, \pi]$		
13:	$z_0 \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand})))$		
14:	for $i = 1 \dots N_{iter}$ do		
15:	$a \leftarrow \mathcal{P}_d(g(z)) $		
16:	$\{z_{i+1}, s_{i+1}\} \leftarrow \{z_i, s_i\} - \alpha \nabla \mathcal{L}_a(s_i \cdot a, a_{target})$		
17:	end for		
18:	$\mathbf{return} \ slm_j \leftarrow g(z)$		
19:	end for		
Alc	gorithm 2 DOF-ont B-SGD		
1:	N : Number of focal states		
2:	γ : Regularization coefficient		
2: 3:	γ : Regularization coefficient coherent_recon(\cdot , ΔD) : Intensity in coherent imaging / Eq.4		
2: 3: 4:	γ : Regularization coefficient coherent_recon(\cdot , ΔD) : Intensity in coherent imaging / Eq.4 incoherent_recon(\cdot , ΔD) : Intensity in incoherent imaging / Eq.6		
2: 3: 4: 5:	γ : Regularization coefficient coherent_recon(\cdot , ΔD) : Intensity in coherent imaging / Eq.4 incoherent_recon(\cdot , ΔD) : Intensity in incoherent imaging / Eq.6 $CR_{\mathcal{S}}(\cdot)$: Contrast ratio estimated in frequency band \mathcal{S} / Eq.5		
2: 3: 4: 5: 6:	γ : Regularization coefficient coherent_recon(\cdot , ΔD) : Intensity in coherent imaging / Eq.4 incoherent_recon(\cdot , ΔD) : Intensity in incoherent imaging / Eq.6 $CR_{\mathcal{S}}(\cdot)$: Contrast ratio estimated in frequency band \mathcal{S} / Eq.5 $\mathcal{L}_{CR}(\cdot, \cdot)$: l_1 loss of contrast ratio		
2: 3: 4: 5: 6: 7:	$\begin{array}{l} \gamma: \operatorname{Regularization coefficient} \\ \operatorname{coherent_recon}(\cdot, \Delta D) : \operatorname{Intensity} \text{ in coherent imaging / Eq.4} \\ \operatorname{incoherent_recon}(\cdot, \Delta D) : \operatorname{Intensity} \text{ in incoherent imaging / Eq.6} \\ \operatorname{CR}_{\mathcal{S}}(\cdot) : \operatorname{Contrast ratio estimated in frequency band } \mathcal{S} / \operatorname{Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio} \\ a_{target} \leftarrow \operatorname{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \end{array}$		
2: 3: 4: 5: 6: 7: 8:	$\gamma : \text{Regularization coefficient}$ $\text{coherent_recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4}$ $\text{incoherent_recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6}$ $CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5}$ $\mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio}$ $a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})}$ $\text{for } j = 1 \dots J \text{ do}$		
2: 3: 4: 5: 6: 7: 8: 9:	$\gamma : \text{Regularization coefficient}$ $\text{coherent_recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4}$ $\text{incoherent_recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6}$ $CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5}$ $\mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio}$ $a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})}$ $\text{for } j = 1 \dots J \text{ do}$ $\phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi]$		
2: 3: 4: 5: 6: 7: 8: 9: 10:	$\gamma : \text{Regularization coefficient}$ $\text{coherent_recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4}$ $\text{incoherent_recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6}$ $CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5}$ $\mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio}$ $a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})}$ $\text{for } j = 1 \dots J \text{ do}$ $\phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi]$ $z_0 \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand})))$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11:	$\begin{aligned} \gamma : & \text{Regularization coefficient} \\ & \text{coherent_recon}(\cdot, \Delta D) : & \text{Intensity in coherent imaging / Eq.4} \\ & \text{incoherent_recon}(\cdot, \Delta D) : & \text{Intensity in incoherent imaging / Eq.6} \\ & CR_{\mathcal{S}}(\cdot) : & \text{Contrast ratio estimated in frequency band } \mathcal{S} / & \text{Eq.5} \\ & \mathcal{L}_{CR}(\cdot, \cdot) : & l_1 & \text{loss of contrast ratio} \\ & a_{target} \leftarrow & \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ & \text{for } j = 1 \dots J \text{ do} \\ & \phi_{rand} \leftarrow & \text{Initialize phase in a range of } (-\pi, \pi] \\ & z_0 \leftarrow \mathcal{P}_{-d} & (\text{band_limit}(a_{target} \cdot \phi_{rand}))) \\ & \text{for } i = 1 \dots N_{iter} \text{ do} \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12:	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent_recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent_recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_0 \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_d(q(z)) \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13:	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent_recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent_recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_0 \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_d (g(z)) \\ u \leftarrow s \cdot \mathcal{P}_d (g(z)) \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14:	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent_recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent_recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_0 \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_d (g(z)) \\ u \leftarrow s \cdot \mathcal{P}_d (g(z)) \\ \log s_{cr} \leftarrow 0 \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14: 15:	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent_recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent_recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_0 \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_d(g(z)) \\ u \leftarrow s \cdot \mathcal{P}_d(g(z)) \\ \text{loss}_{cr} \leftarrow 0 \\ \text{for } n = 1 \dots N \text{ do} \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14: 15: 16:	$\gamma : \text{Regularization coefficient}$ $coherent_recon(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4}$ incoherent_recon(\cdot, \Delta D) : Intensity in incoherent imaging / Eq.6 $CR_{S}(\cdot) : \text{Contrast ratio estimated in frequency band } S / \text{Eq.5}$ $\mathcal{L}_{CR}(\cdot, \cdot) : l_{1} \text{ loss of contrast ratio}$ $a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})}$ for $j = 1 \dots J$ do $\phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi]$ $z_{0} \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand})))$ for $i = 1 \dots N_{iter}$ do $a \leftarrow \mathcal{P}_{d}(g(z)) $ $u \leftarrow s \cdot \mathcal{P}_{d}(g(z))$ $loss_{cr} \leftarrow 0$ for $n = 1 \dots N$ do $(r_{rate} = CR s(\Gamma(\text{coherent} \operatorname{recon}(u \land D_{r}))))$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14: 15: 15: 17:	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent}_\text{recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent}_\text{recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_0 \leftarrow \mathcal{P}_{-d} (\text{band}_\text{limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_d(g(z)) \\ u \leftarrow s \cdot \mathcal{P}_d(g(z)) \\ \log s_{cr} \leftarrow 0 \\ \text{for } n = 1 \dots N \text{ do} \\ cr_{ch} = CR_{\mathcal{S}}(\Gamma(\text{coherent}_\text{recon}(u, \Delta D_n))) \\ cr_{it} = CR \leq (\text{incoherent}_\text{recon}(I_{target} \cdot \Delta D_n)) \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14: 15: 16: 17: 12: 14: 14: 14: 15: 14: 14: 14: 14: 14: 14: 14: 14	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent_recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent_recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_{S}(\cdot) : \text{Contrast ratio estimated in frequency band S / Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_{1} \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_{0} \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_{d}(g(z)) \\ u \leftarrow s \cdot \mathcal{P}_{d}(g(z)) \\ \log s_{cr} \leftarrow 0 \\ \text{for } n = 1 \dots N \text{ do} \\ cr_{ch} = CR_{S}(\Gamma(\text{coherent_recon}(u, \Delta D_{n}))) \\ cr_{ih} = CR_{S}(\text{incoherent_recon}(I_{target}, \Delta D_{n})) \\ \log s_{cr} \leftarrow \log s_{cr} + \frac{Y}{2} \int_{\Omega} c_{cr}(s_{cr} + cr_{cr}) \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14: 15: 16: 17: 18: 19: 10: 11: 12: 14: 14: 14: 14: 15: 14: 14: 14: 14: 14: 14: 14: 14	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent}_\text{recon}(, \Delta D) : \text{Intensity in coherent imaging} / \text{Eq.4} \\ \text{incoherent}_\text{recon}(, \Delta D) : \text{Intensity in incoherent imaging} / \text{Eq.6} \\ CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_0 \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_d (g(z)) \\ u \leftarrow s \cdot \mathcal{P}_d (g(z)) \\ loss_{cr} \leftarrow 0 \\ \text{for } n = 1 \dots N \text{ do} \\ cr_{ch} = CR_{\mathcal{S}}(\Gamma(\text{coherent_recon}(u, \Delta D_n))) \\ cr_{ih} = CR_{\mathcal{S}}(\text{incoherent_recon}(I_{target}, \Delta D_n)) \\ loss_{cr} \leftarrow \log_{cr} + \frac{\gamma}{N} \mathcal{L}_{CR}(cr_{ch}, cr_{ih}) \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14: 15: 16: 17: 18: 19: 20: 20: 20: 20: 20: 20: 20: 20	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent_recon}(\cdot, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent_recon}(\cdot, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_{\mathcal{S}}(\cdot) : \text{Contrast ratio estimated in frequency band } \mathcal{S} / \text{Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_0 \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_d (g(z)) \\ u \leftarrow s \cdot \mathcal{P}_d (g(z)) \\ loss_{cr} \leftarrow 0 \\ \text{for } n = 1 \dots N \text{ do} \\ cr_{ch} = CR_{\mathcal{S}}(\Gamma(\text{coherent_recon}(u, \Delta D_n))) \\ cr_{ih} = CR_{\mathcal{S}}(\text{incoherent_recon}(l_{target}, \Delta D_n)) \\ loss_{cr} \leftarrow loss_{cr} + \frac{Y}{N} \mathcal{L}_{CR}(cr_{ch}, cr_{ih}) \\ \text{end for} \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14: 15: 16: 17: 18: 19: 20: 21:	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent_recon}(, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent_recon}(, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_S(\cdot) : \text{Contrast ratio estimated in frequency band S / Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_1 \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_0 \leftarrow \mathcal{P}_{-d} (\text{band_limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_d (g(z)) \\ u \leftarrow s \cdot \mathcal{P}_d (g(z)) \\ loss_{cr} \leftarrow 0 \\ \text{for } n = 1 \dots N \text{ do} \\ cr_{ch} = CR_S(\Gamma(\text{coherent_recon}(u,\Delta D_n))) \\ cr_{ih} = CR_S(\text{incoherent_recon}(I_{target},\Delta D_n)) \\ loss_{cr} \leftarrow loss_{cr} + \frac{N}{N} \mathcal{L}_{CR}(cr_{ch}, cr_{ih}) \\ \text{end for} \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14: 15: 16: 17: 18: 19: 20: 21: 22:	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent}_\text{recon}(, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent}_\text{recon}(, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_{S}(\cdot) : \text{Contrast ratio estimated in frequency band S / Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_{1} \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_{0} \leftarrow \mathcal{P}_{-d} (\text{band}_\text{limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_{d}(g(z)) \\ u \leftarrow s \cdot \mathcal{P}_{d}(g(z)) \\ loss_{cr} \leftarrow 0 \\ \text{for } n = 1 \dots N \text{ do} \\ cr_{ch} = CR_{S}(\Gamma(\text{coherent}_\text{recon}(u,\Delta D_{n}))) \\ cr_{ih} = CR_{S}(\text{incoherent}_\text{recon}(I_{target},\Delta D_{n})) \\ loss_{cr} \leftarrow loss_{cr} + \frac{N}{N} \mathcal{L}_{CR}(cr_{ch}, cr_{ih}) \\ \text{end for} \\ \text{end for} \\ \{z_{i+1}, s_{i+1}\} \leftarrow \{z_{i}, s_{i}\} - \alpha \nabla (\mathcal{L}_{a}(s_{i} \cdot a, a_{target}) + loss_{cr}) \\ \text{rature she is } a(a) \end{aligned}$		
2: 3: 4: 5: 6: 7: 8: 9: 10: 11: 12: 13: 14: 15: 16: 17: 18: 19: 20: 21: 22: 22:	$\begin{aligned} \gamma : \text{Regularization coefficient} \\ \text{coherent}_\text{recon}(, \Delta D) : \text{Intensity in coherent imaging / Eq.4} \\ \text{incoherent}_\text{recon}(, \Delta D) : \text{Intensity in incoherent imaging / Eq.6} \\ CR_{S}(\cdot) : \text{Contrast ratio estimated in frequency band S / Eq.5} \\ \mathcal{L}_{CR}(\cdot, \cdot) : l_{1} \text{ loss of contrast ratio} \\ a_{target} \leftarrow \text{Load target amplitude with } \sqrt{\Gamma^{-1}(I_{target})} \\ \text{for } j = 1 \dots J \text{ do} \\ \phi_{rand} \leftarrow \text{Initialize phase in a range of } (-\pi, \pi] \\ z_{0} \leftarrow \mathcal{P}_{-d}(\text{band}_\text{limit}(a_{target} \cdot \phi_{rand}))) \\ \text{for } i = 1 \dots N_{iter} \text{ do} \\ a \leftarrow \mathcal{P}_{d}(g(z)) \\ u \leftarrow s \cdot \mathcal{P}_{d}(g(z)) \\ loss_{cr} \leftarrow 0 \\ \text{for } n = 1 \dots N \text{ do} \\ cr_{ch} = CR_{S}(\Gamma(\text{coherent}_\text{recon}(u, \Delta D_{n}))) \\ cr_{ih} = CR_{S}(\text{incoherent}_\text{recon}(I_{target}, \Delta D_{n})) \\ loss_{cr} \leftarrow loss_{cr} + \frac{\gamma}{N} \mathcal{L}_{CR}(cr_{ch}, cr_{ih}) \\ \text{ end for} \\ \{z_{i+1}, s_{i+1}\} \leftarrow \{z_{i}, s_{i}\} - \alpha \nabla(\mathcal{L}_{a}(s_{i} \cdot a, a_{target}) + loss_{cr}) \\ \text{return } slm_{j} \leftarrow g(z) \end{aligned}$		

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	12	Dongyeon Kim, Seung-Woo Nam, Byounghyo Lee, Jong-Mo Seo, and Byoungho Lee
573	 B. Lee, D. Kim, S. Lee, C. Chen, and B. Lee. High-contrast, speckle-free, true 3d holography via binary cgh optimization. Scientific Reports, 12(1):28 2022. ISSN 2045-2322. doi: 10.1038/s41598-022-06405-2. URL https://doi.org/10.1038/s41598-022-06405-2. V. Peng, S. Choi, N. Padmanaban, and G. Watzstein, Neural holography with camera-in-the-loop training. ACM Trans. Graph. 39(6), ppy 2020. 	
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